

# Using PDEs to Calculate Optimal Foot Motion for Walking

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CE C291F: Control and optimization of distributed systems

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# Outline

- Research project background
- Approach for distributed system
  - Hybrid systems
- PDE model
  - Compass gait biped
- Implementation of control
  - Human motion data
- Refinements of model

# Project Background

- Motivation
  - Quantitative Parkinson's disease diagnosis
- Inertial measurement units for human movement analysis
  - Wireless Lagrangian sensors attached to feet
  - Triaxial accelerometers and gyroscopes
  - Gait analysis



# Problem Statement

- Distributed system
  - Data collection along trajectory
  - Multiple parameters (position, velocity, time, etc.)
- PDE to calculate optimal foot motion to take a step during walking

# Approach

- Walking: continuous and discrete dynamics
  - Hybrid systems
  - State consists of vector signals
  - Flow equation  $f(x)$  and jump equation  $g(x)$

# Hybrid Systems

- Simple hybrid system: a 4-tuple

$$H = (D, G, R, f)$$

where

$D \subseteq \mathbf{R}^n$       domain

$G \subset D$       guard

$R: G \rightarrow D$       reset map, from impact equations

$f$       vector field on  $D$ , i.e.  $\dot{x} = f(x)$

- Simple hybrid control system: a 6-tuple

$$H = (D, U, G, R, f, g)$$

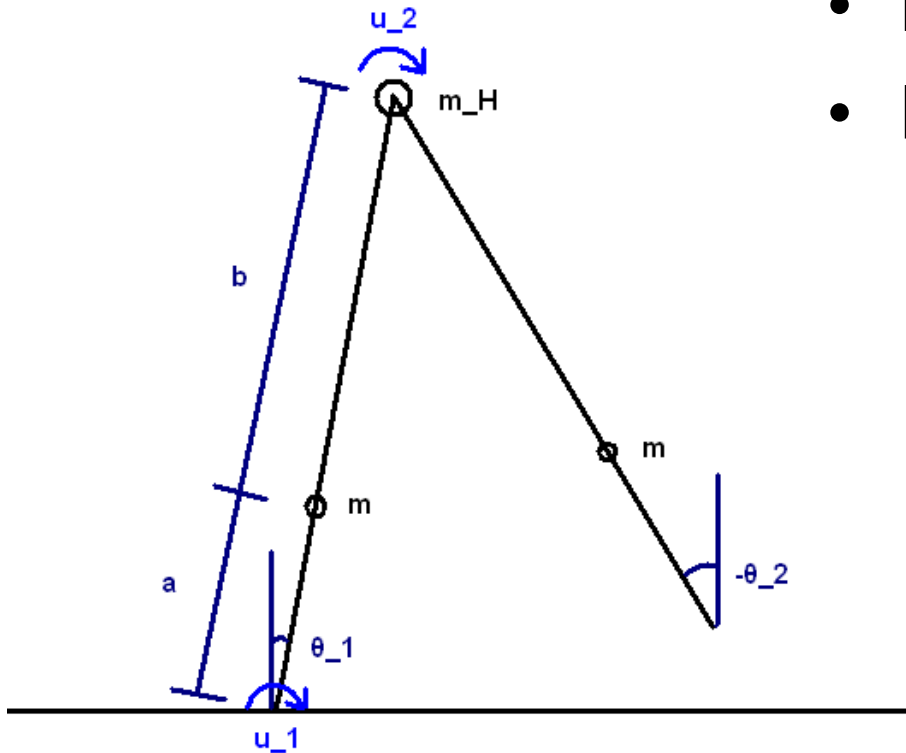
where

$D, G, R$       domain, guard, reset map

$U \subseteq \mathbf{R}^k$       set of admissible controls

$(f, g)$       control system, i.e.  $\dot{x} = f(x) + g(x)u$

# Compass Gait Biped Model



- From robotics and control
- Parameters of model

$m, m_H$  masses of limbs, hip

$a, b$  length of limbs

$\theta = \begin{bmatrix} \theta_1 \\ \theta_2 \end{bmatrix}$  angle vector

$u = \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$  control torque vector

# Langrangian Dynamics

- Langrangian of compass gait biped model

$$L(\theta, \dot{\theta}) = \frac{1}{2} \dot{\theta}^T M(\theta) \dot{\theta} - P(\theta)$$

where

$M(\theta)$  inertial matrix, i.e.  $\frac{1}{2} \dot{\theta}^T M(\theta) \dot{\theta}$  kinetic energy

$P(\theta)$  potential energy

- Controlled Euler-Lagrange equations

$$M(\theta) \ddot{\theta} + C(\theta, \dot{\theta}) \dot{\theta} + G(\theta) = Su$$

where

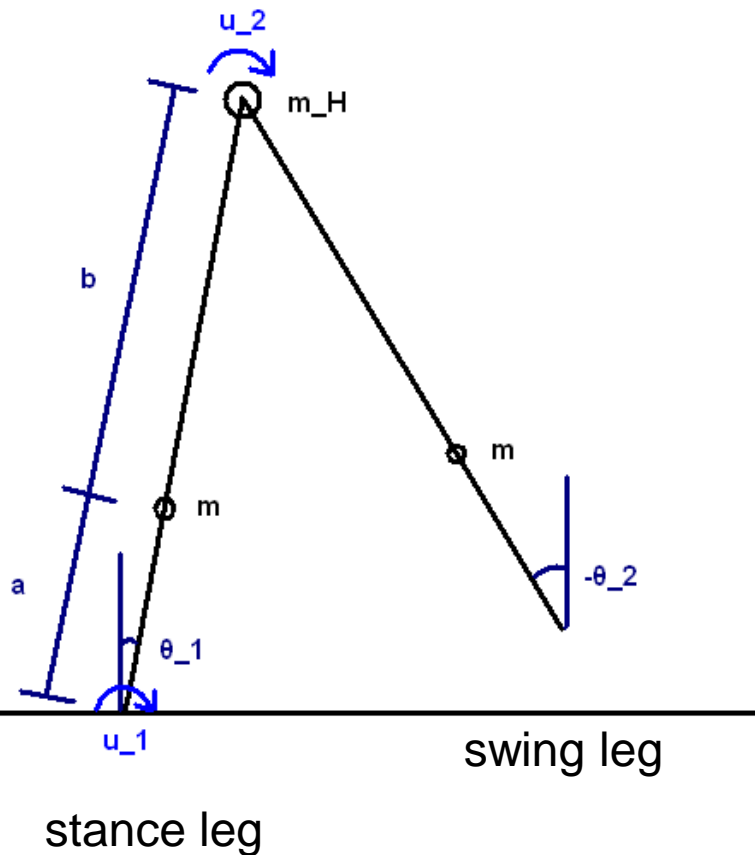
$M(\theta)$  inertial matrix

$C(\theta, \dot{\theta})$  coriolis matrix

$$G(\theta) = \frac{\partial P}{\partial \theta}(\theta)$$



# Simple Hybrid Mechanical Control System



constraint function  $V(\theta) = \cos \theta_1 - \cos \theta_2$

SHMCS a 6-tuple

$$H = (D, U, G, R, f, g)$$

where

$$D = \left\{ \begin{bmatrix} \theta \\ \dot{\theta} \end{bmatrix} \in \mathbf{R}^4 : V(\theta) \geq 0 \right\}$$

$$G = \left\{ \begin{bmatrix} \theta \\ \dot{\theta} \end{bmatrix} \in \mathbf{R}^4 : V(\theta) = 0, \left[ \frac{\partial V}{\partial \theta}(\theta) \right]^T \dot{\theta} < 0 \right\}$$

$R$  from kinematic constraint function

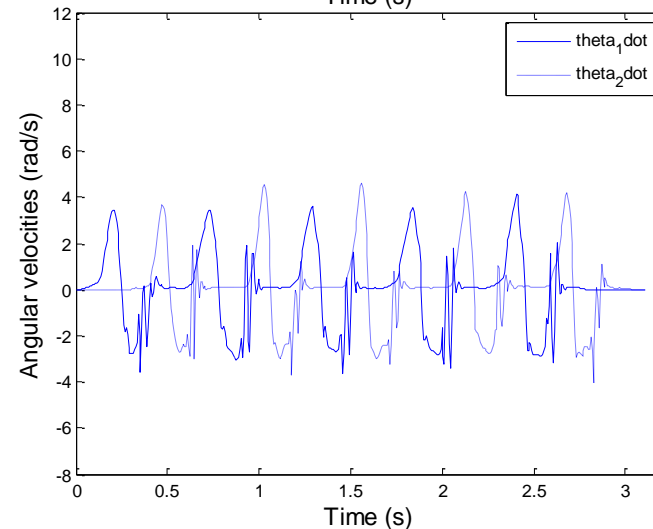
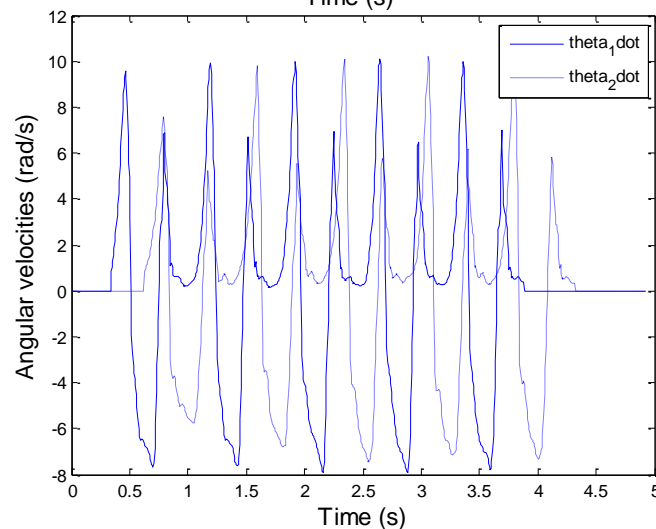
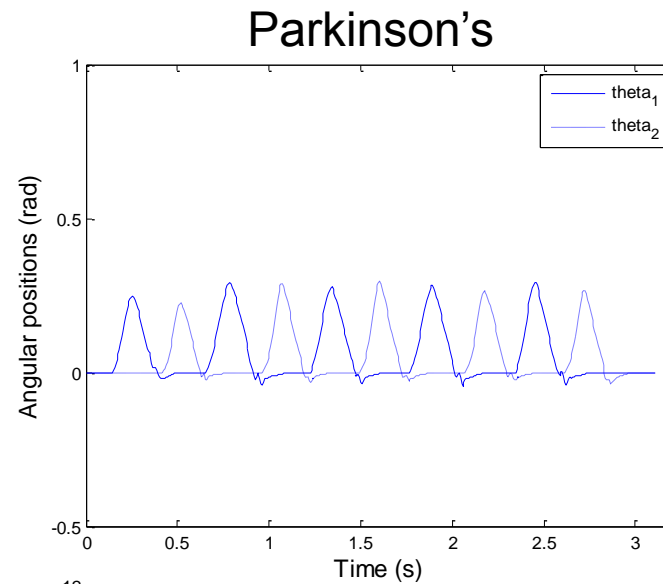
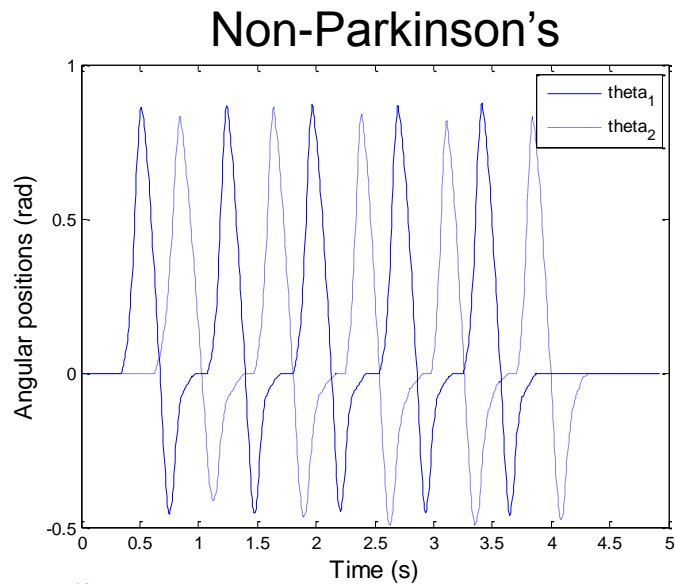
$$U = \mathbf{R}^2$$

$$f(\theta, \dot{\theta}) = \begin{bmatrix} \dot{\theta} \\ M(\theta)^{-1}(-C(\theta, \dot{\theta})\dot{\theta} - G(\theta)) \end{bmatrix}$$

$$g(\theta, \dot{\theta}) = \begin{bmatrix} 0_{2 \times 2} \\ M(\theta)^{-1}S \end{bmatrix}$$

# Implementation of Control: $\theta$ and $\dot{\theta}$

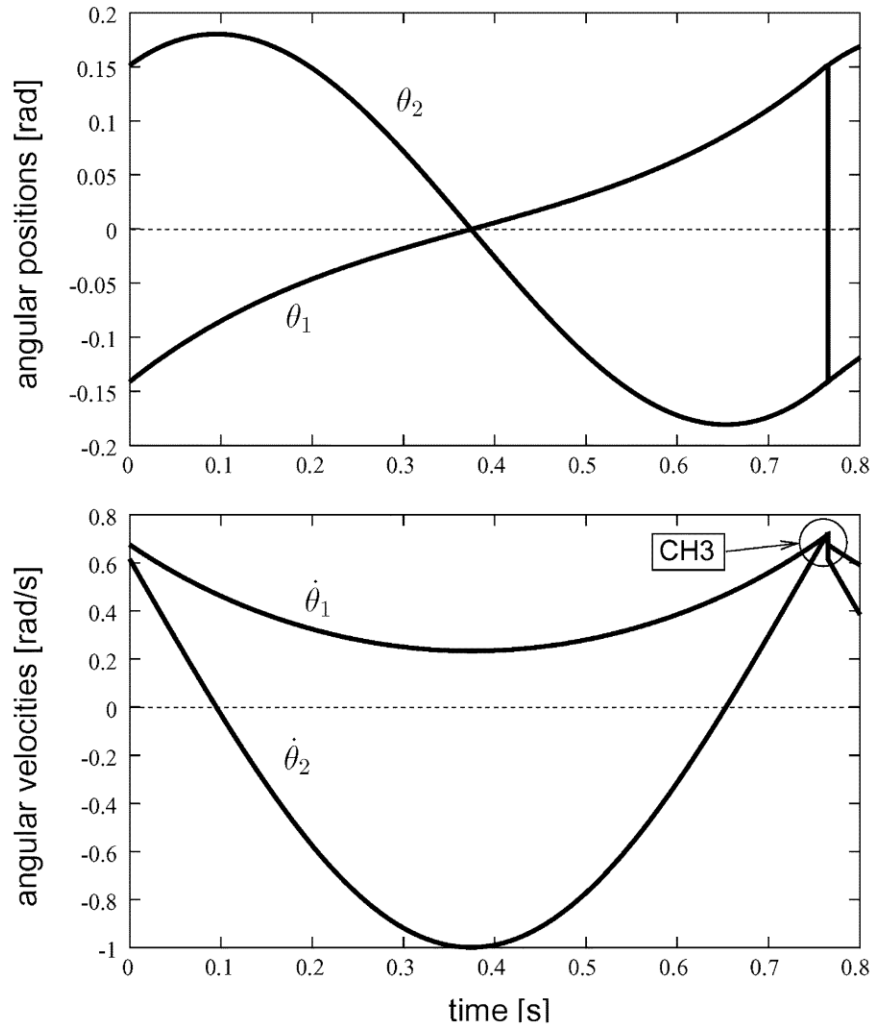
- Experimental human motion data (five cycles)



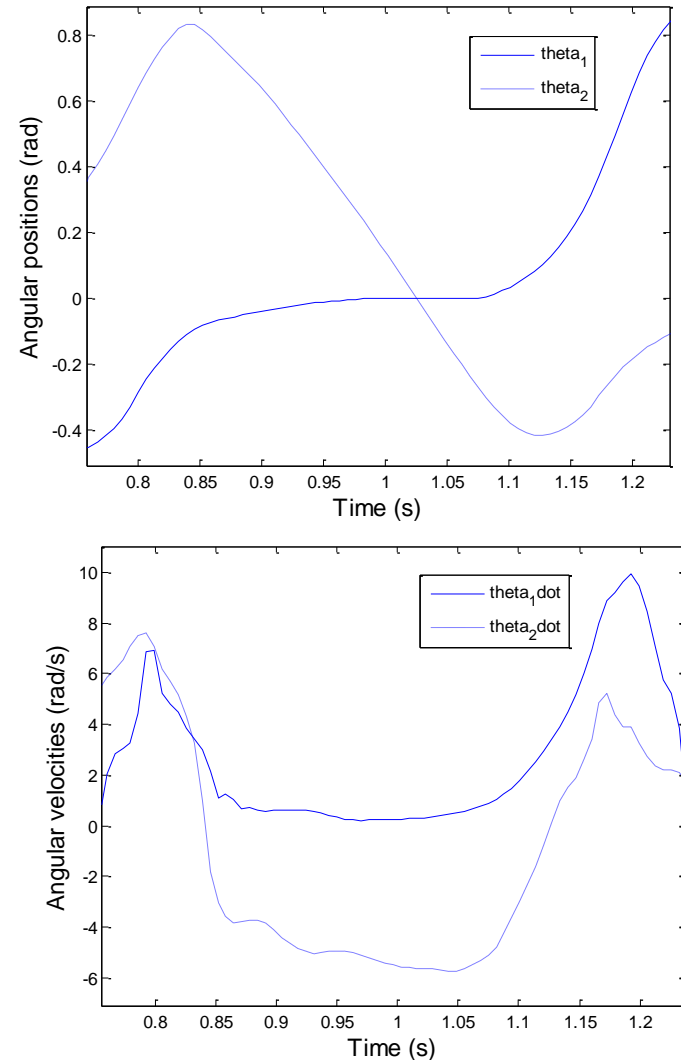
# Comparison with Biped Model: $\theta$ and $\dot{\theta}$

- One cycle (reference for left figures: Asano, 2004)

Biped Model



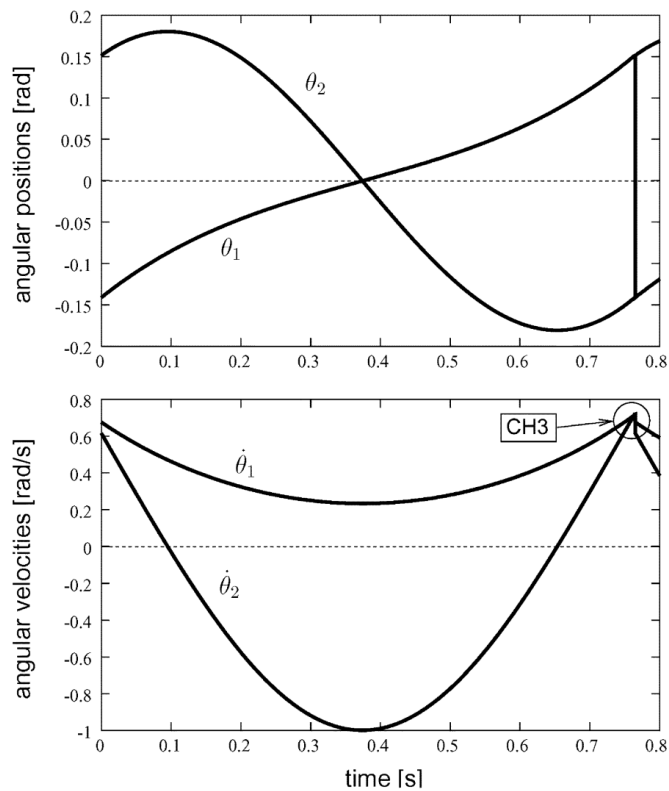
Non-Parkinson's



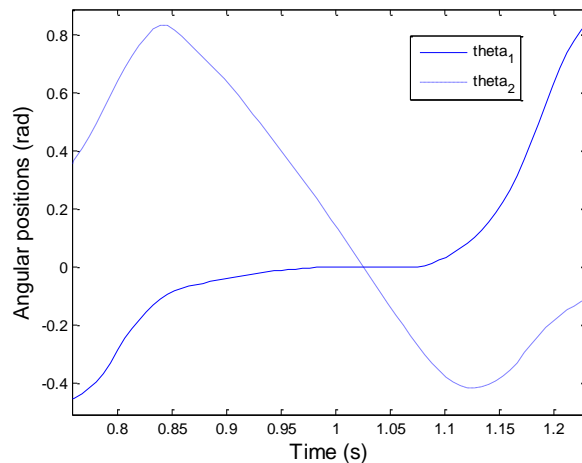
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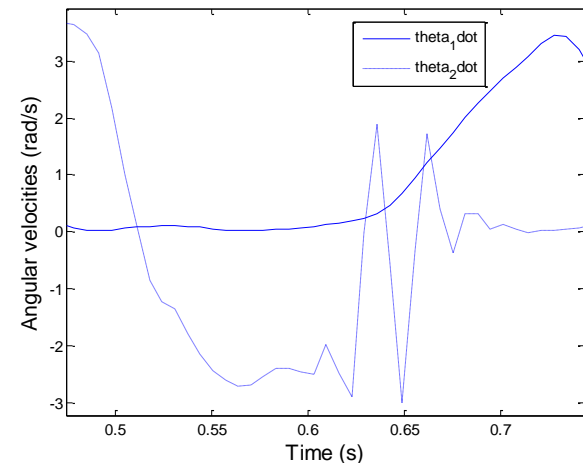
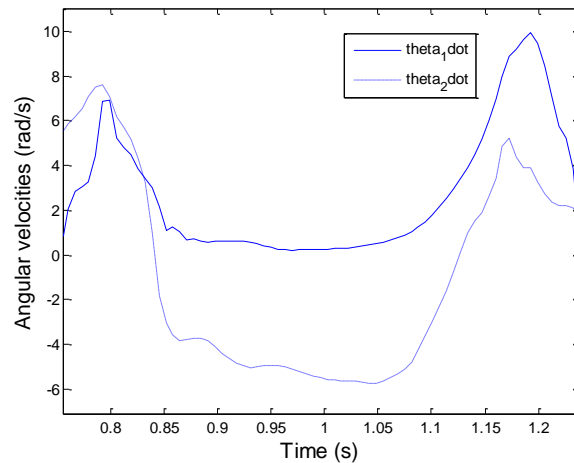
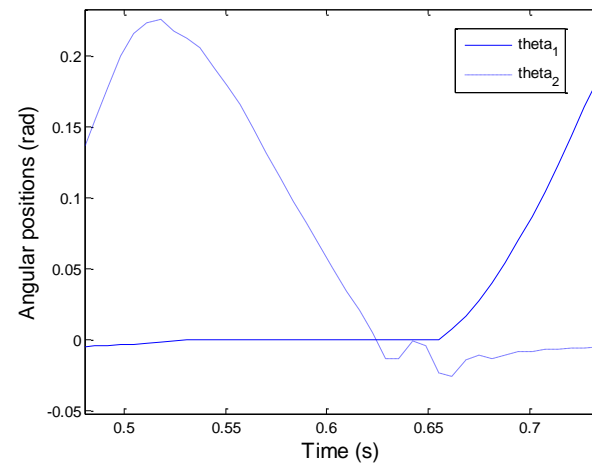
Biped Model



Non-Parkinson's



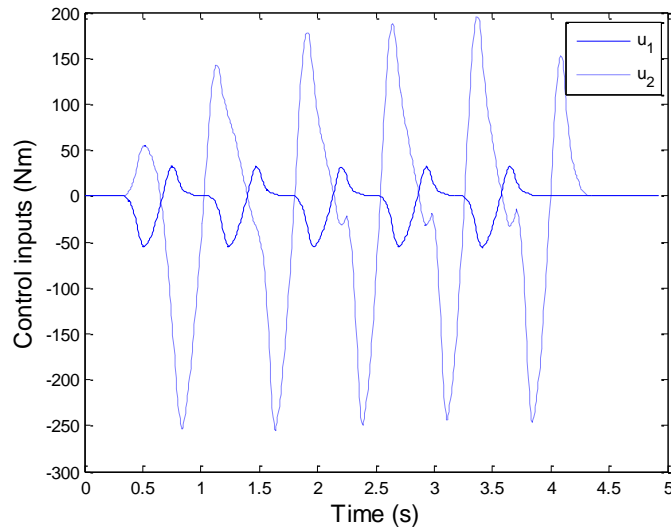
Parkinson's



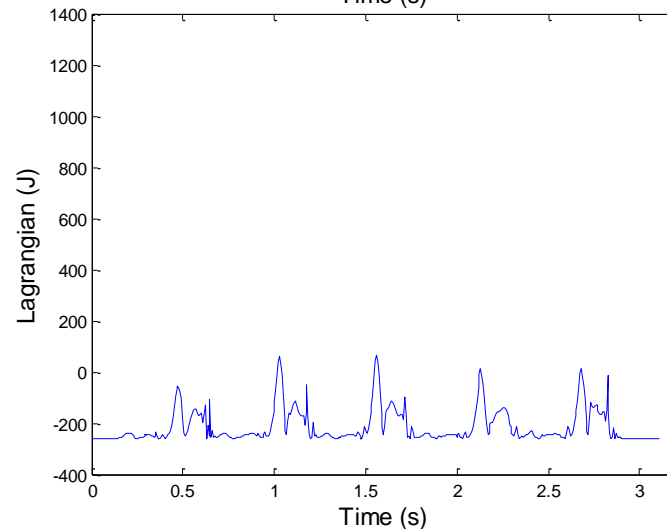
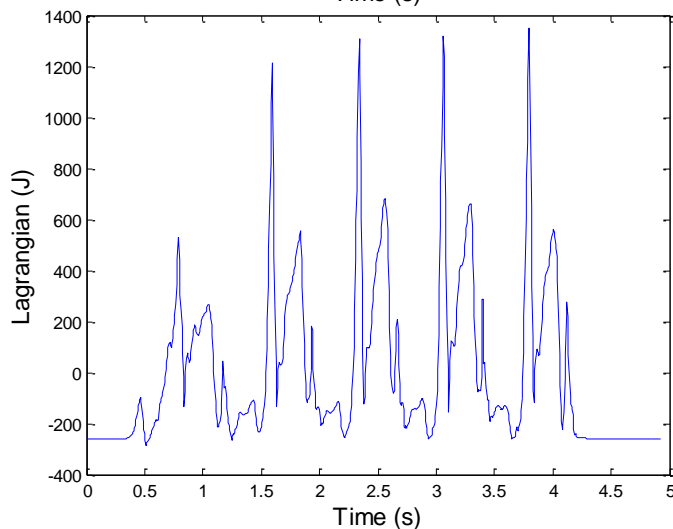
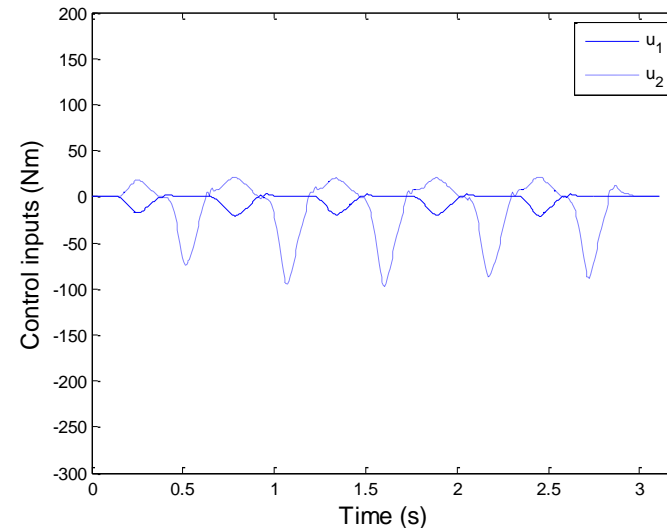
# Implementation of Control: $u$ and $L$

- Experimental human motion data (five cycles)

Non-Parkinson's



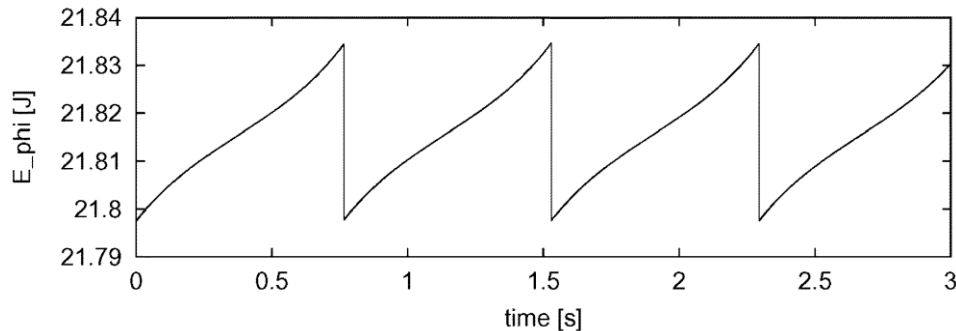
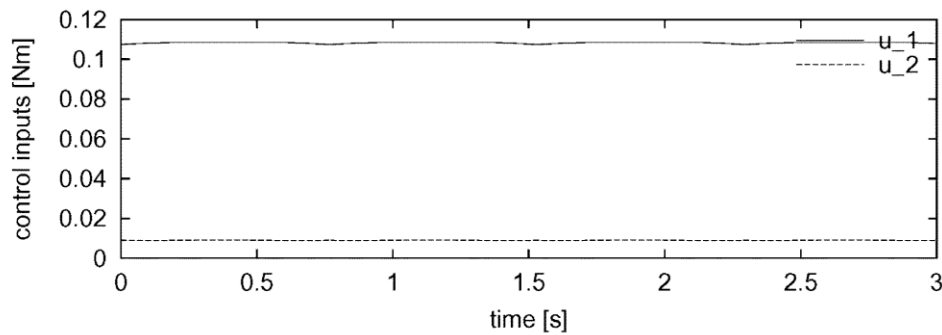
Parkinson's



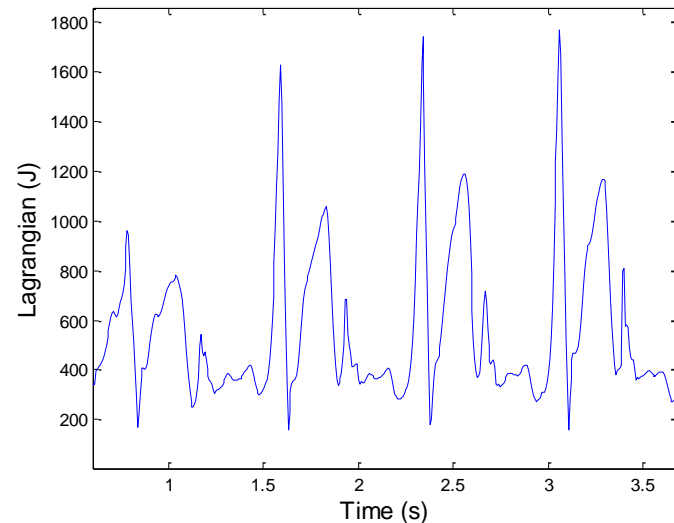
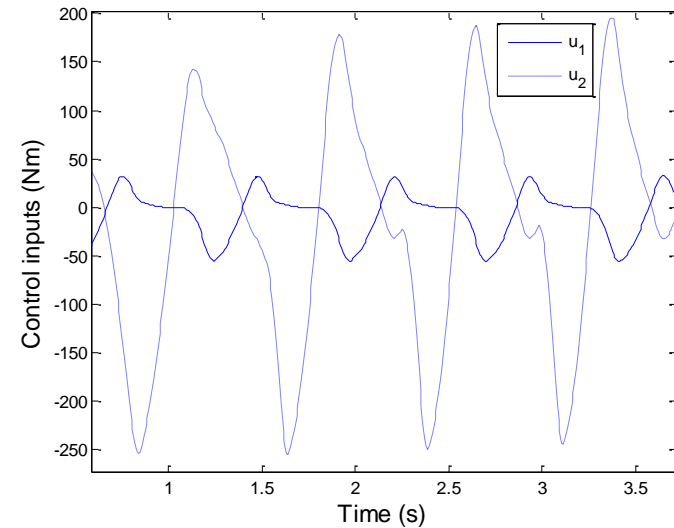
# Comparison with Biped Model: $u$ and $L$

- **Four cycles** (reference for left figures: Asano, 2004)

Biped Model



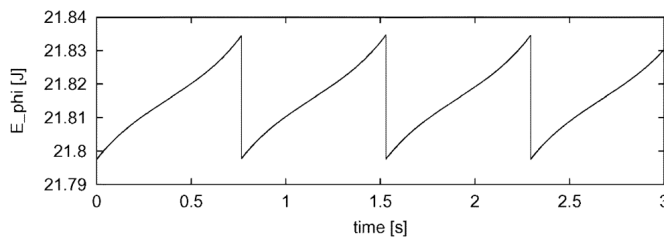
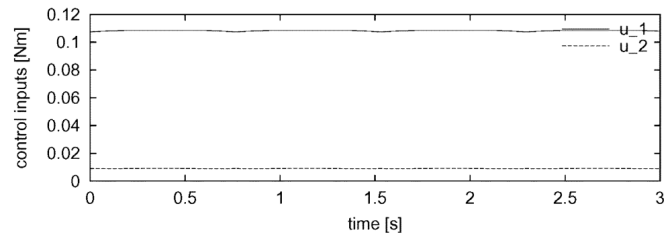
Non-Parkinson's



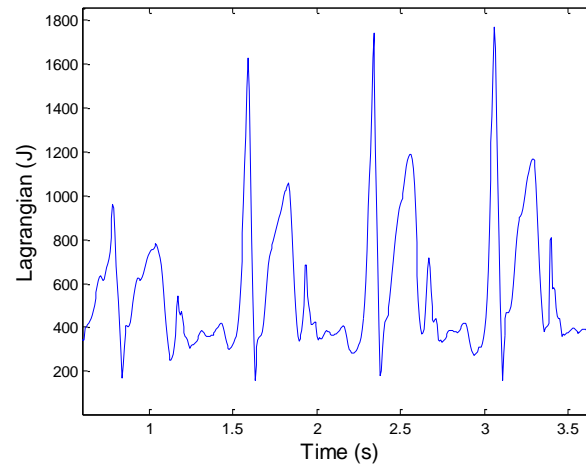
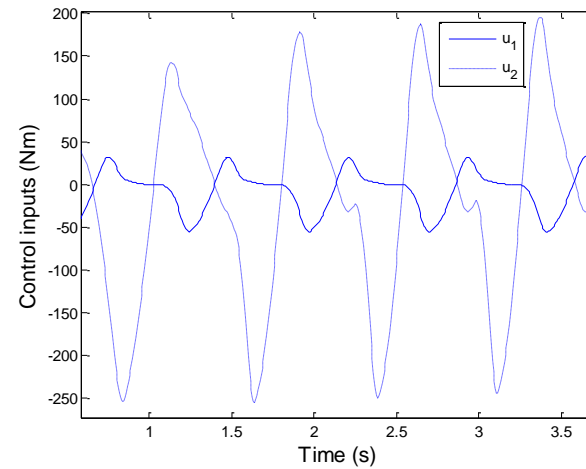
# Comparison with Biped Model: $u$ and $L$

- Four cycles (reference for left figures: Asano, 2004)

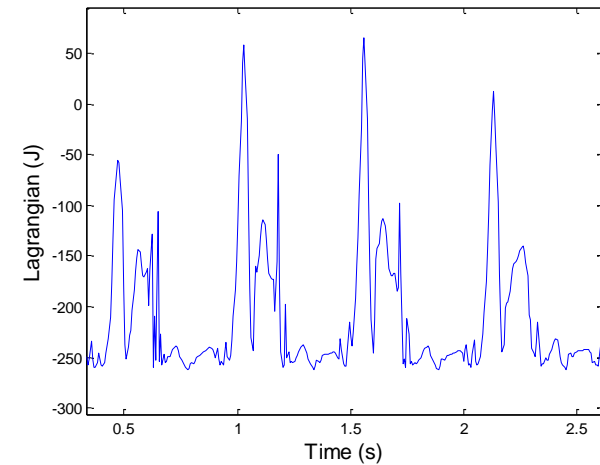
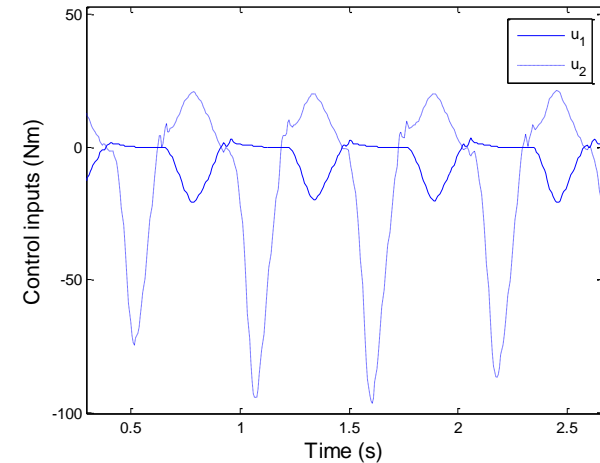
Biped Model



Non-Parkinson's



Parkinson's



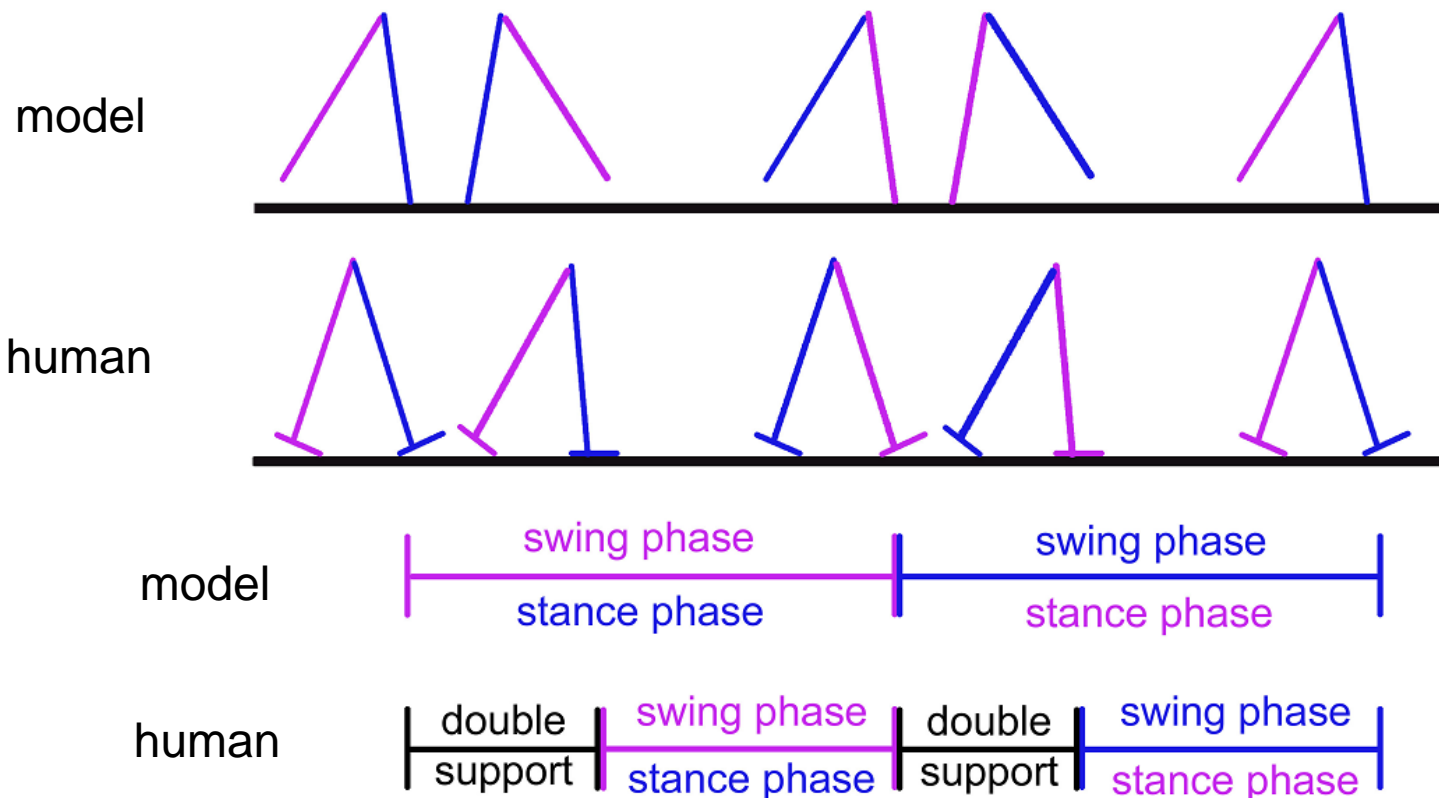
# Refinements of Model

- Assumptions of biped model:
  - Impacts are perfectly inelastic (no bounce)
  - No slipping of the stance leg at ground contact
  - Transfer of support between swing and stance legs is instantaneous, i.e. negligible double support phase



# Refinements of Model Cont'd

- Transfer of support between swing and stance legs is instantaneous, i.e. negligible double support phase



# Summary

- Research project background
  - Quantitative diagnosis of Parkinson's disease
- Approach for distributed system
  - Simple hybrid mechanical control system
- PDE model
  - Compass gait biped
- Implementation of control
  - Human motion data for non-Parkinson's and Parkinson's subjects
- Refinements of model
  - Incorporate double support phase

# References

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