

Parameter Identification for Multimodal Human Motion Measurement

Aaron Bestick, Robert Matthew
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The Problem

Problem

Muscle forces/activation are hard to observe directly

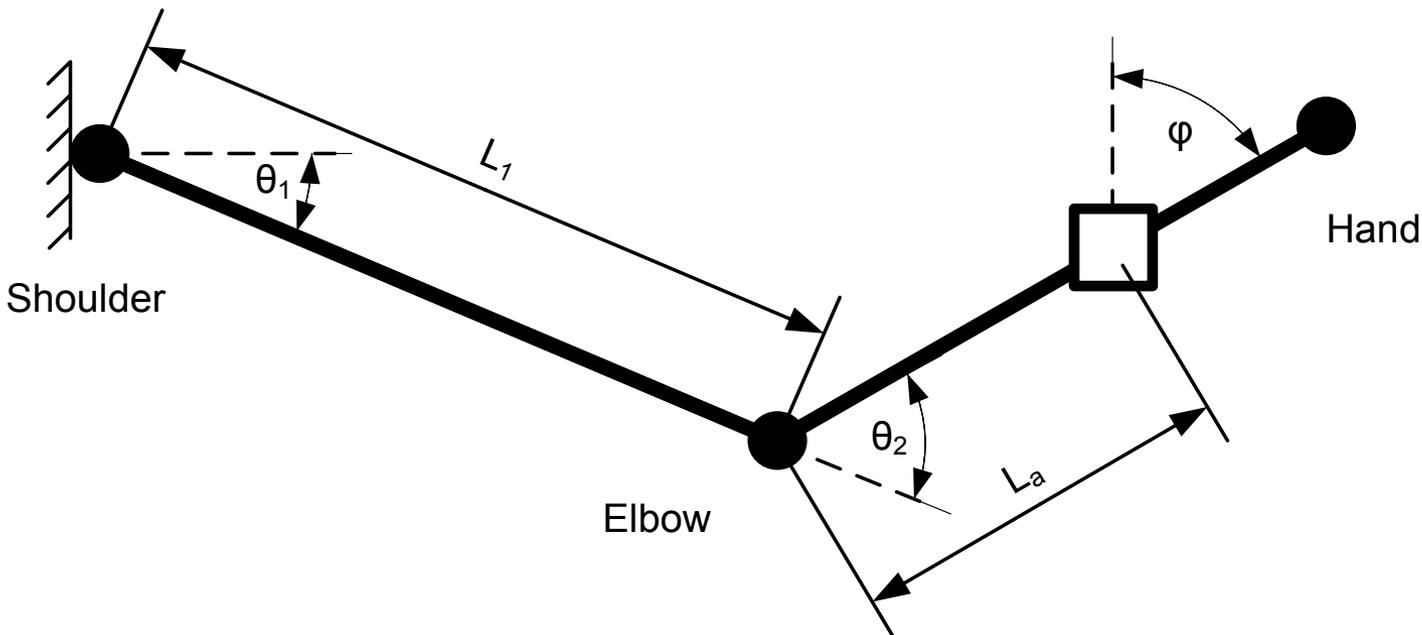
Goal

Infer muscle forces based on easily observed data (motion capture, IMU)

In this project

- Focus on one arm
- Create simplified model of arm
- Extract accurate state information from motion capture + accelerometers
- Combine arm model with state information to infer muscle forces

Mechanical Model



Observed

- θ_1 (mocap)
- θ_2 (mocap)
- Acceleration in sensor coordinates

Want to estimate

- $\dot{\theta}_1$
- $\ddot{\theta}_2$ (joint angular rate/accel)
- $\ddot{\theta}_1$
- θ_2

Parameters to learn

- l (accelerometer position)
- ϕ (accelerometer orientation)

Mathematical Model

Process Model

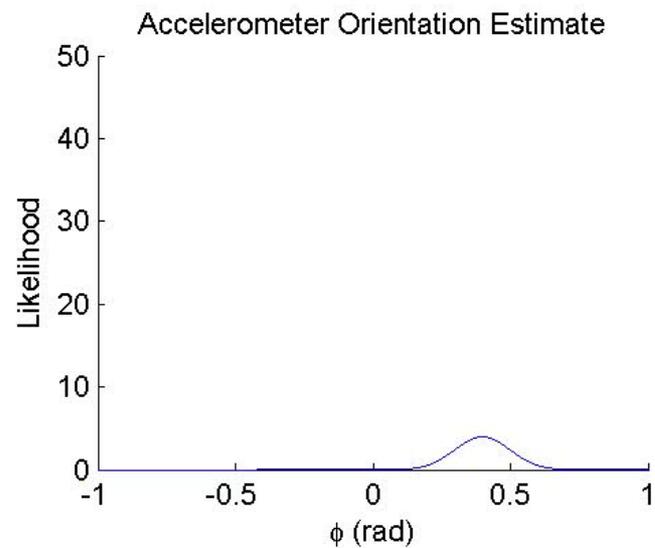
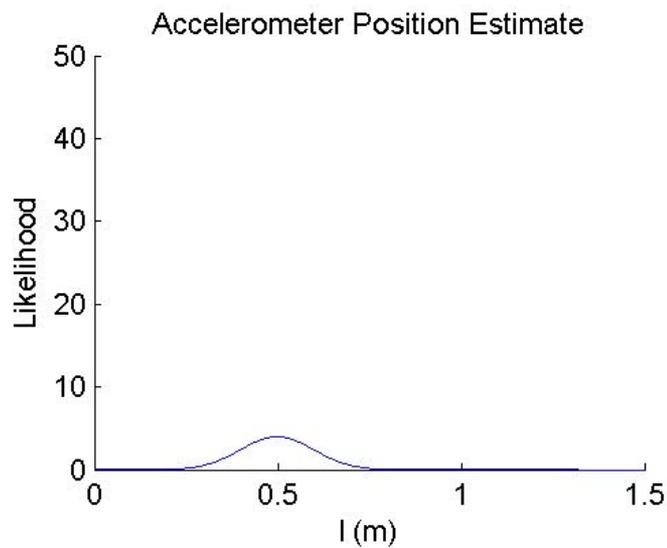
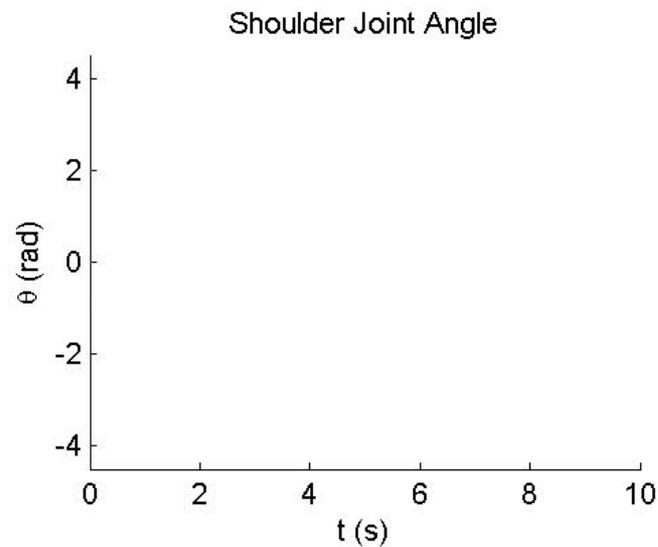
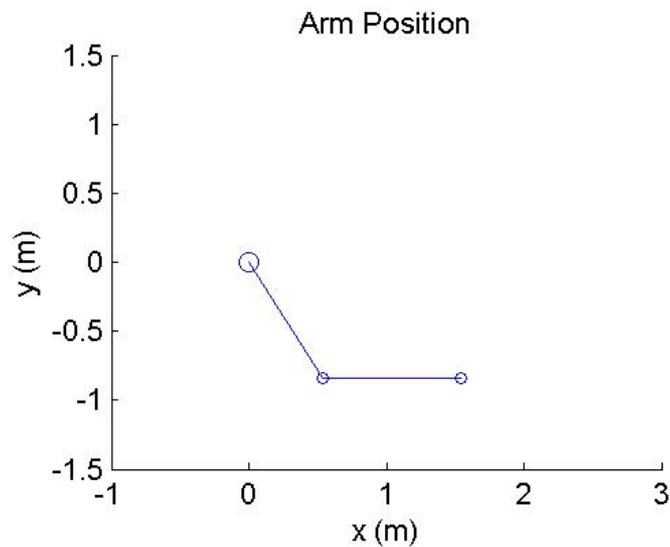
$$\begin{bmatrix} \theta_1 \\ \dot{\theta}_1 \\ \ddot{\theta}_1 \\ \vdots \\ l \\ \varphi \end{bmatrix}_{t+1} = \begin{bmatrix} \theta_1 + T\dot{\theta}_1 + 1/2T^2\ddot{\theta}_1 \\ \dot{\theta}_1 + T\ddot{\theta}_1 \\ \ddot{\theta}_1 + w_{\theta_1} \\ \vdots \\ l + w_l \\ \varphi + w_{\varphi} \end{bmatrix}_t$$

- Constant acceleration process model
- Parameters modeled as a random walk – allows for sensor movement over time
- Noisy measurements of joint angles and acceleration in accelerometer frame

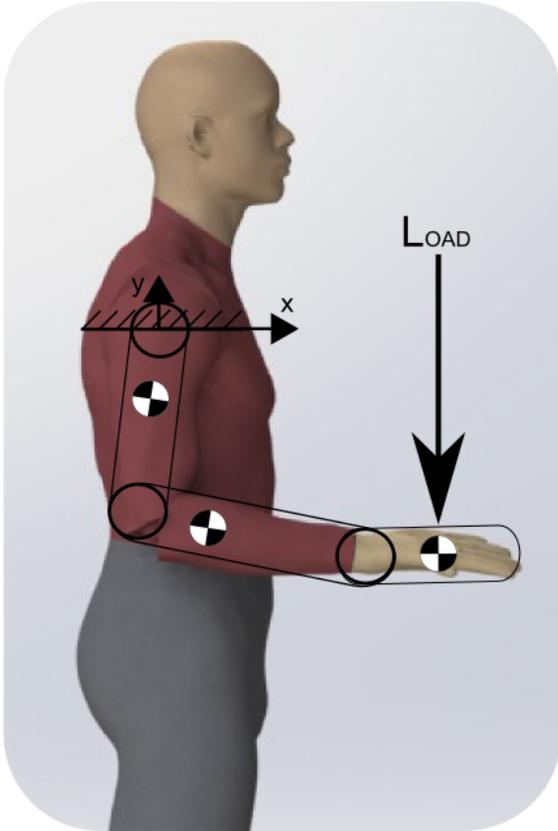
Measurement Model

$$\begin{bmatrix} y_1 \\ y_2 \\ y_3 \\ y_4 \end{bmatrix} = \begin{bmatrix} \theta_1 + \nu_1 \\ \theta_2 + \nu_2 \\ \cos(\theta_1 + \theta_2 + \varphi)(\ddot{x}_a) - \sin(\theta_1 + \theta_2 + \varphi)(\ddot{y}_a) + \nu_3 \\ \sin(\theta_1 + \theta_2 + \varphi)(\ddot{x}_a) + \cos(\theta_1 + \theta_2 + \varphi)(\ddot{y}_a) + \nu_4 \end{bmatrix}$$

Simulation Results: UKF



Experimental Data



Experimental Setup

- Upper body motion capture
- 3-axis accelerometer on forearm
- EMG Sensors

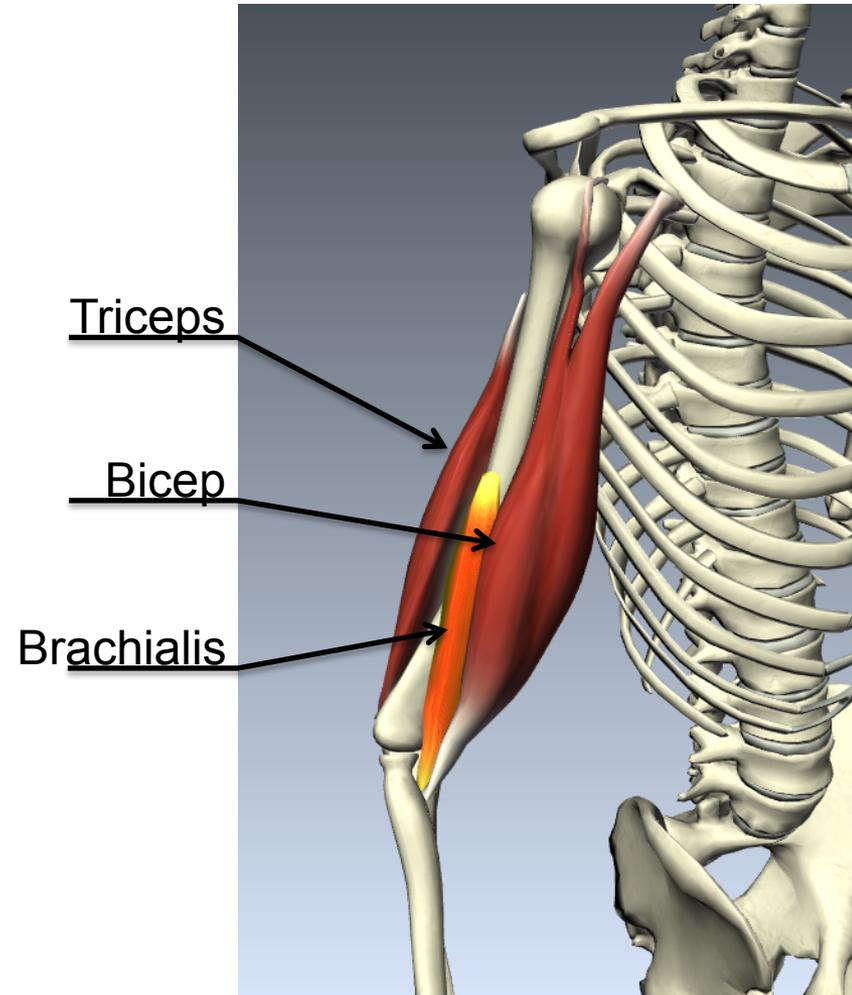
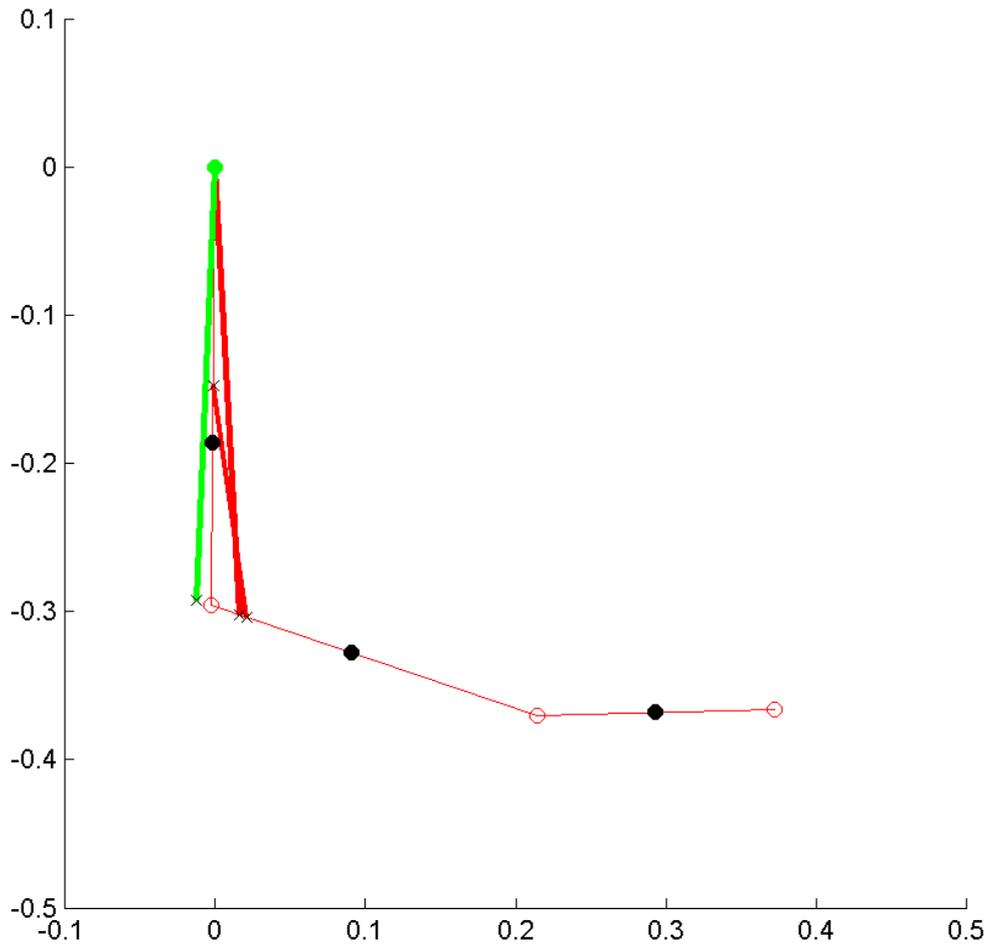
Experiments

1. Planar arm movements
2. 3D arm movements
3. Weight drop tests

Goals

- Test parameter identification on 1-2
- Infer muscle forces in 3

Model: Rigged Skeleton



The head of shortening and the dynamic constants of muscle, A Hill, 1938

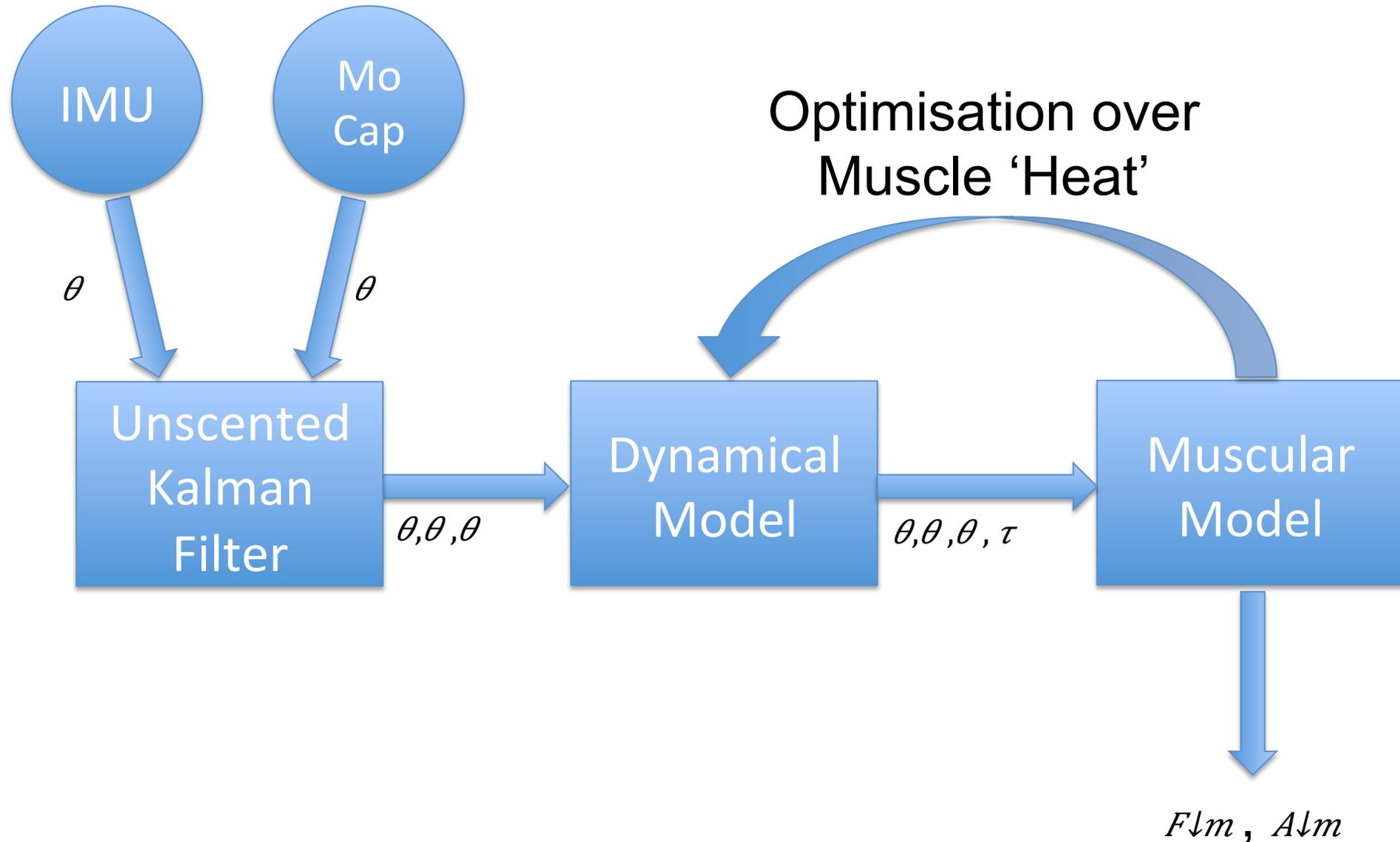
Muscle and Tendon: properties, models, scaling, and application to biomechanics and motor control. F. Zajac, 1989

Biodigital Human. Biodigital Systems 2013. Online: <https://www.biodigitalhuman.com/> Retrieved 2013-04-20.

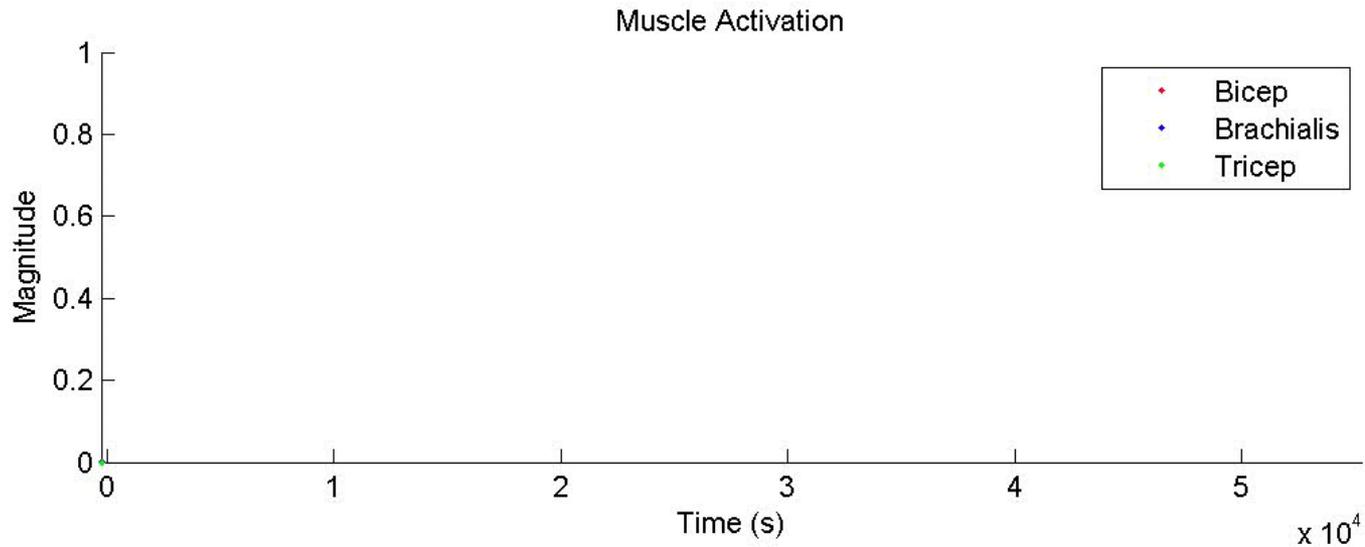
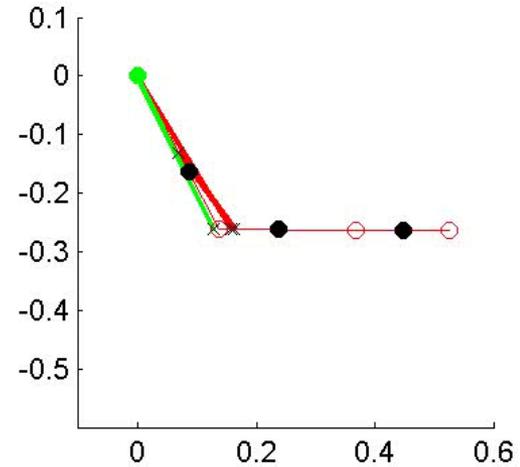
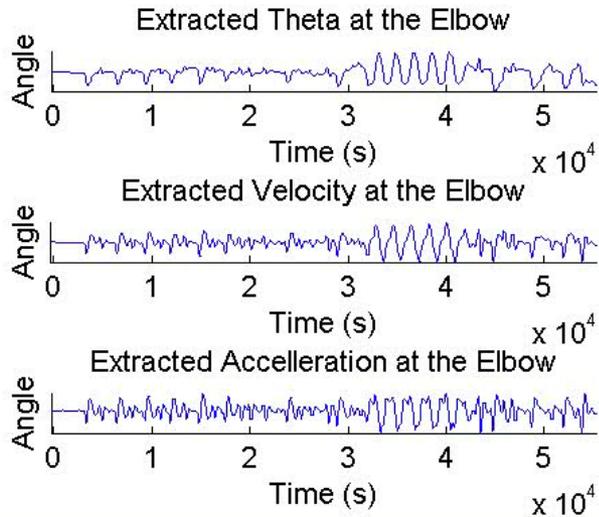
Regularity Aspects in Inverse Musculoskeletal Biomechanics, Marie Lund 2008

Dynamic simulation of human motion: numerically efficient inclusion of muscle physiology by convex optimization, Goele Pipeleers 2008

Entire Process



Arm Motion Video



Remaining Work

Mechanical Modeling

- Extend mechanical model to 3D
- Perform accelerometer localization on a real world dataset
- *Question:* What are the optimal actions for estimating a given parameter?

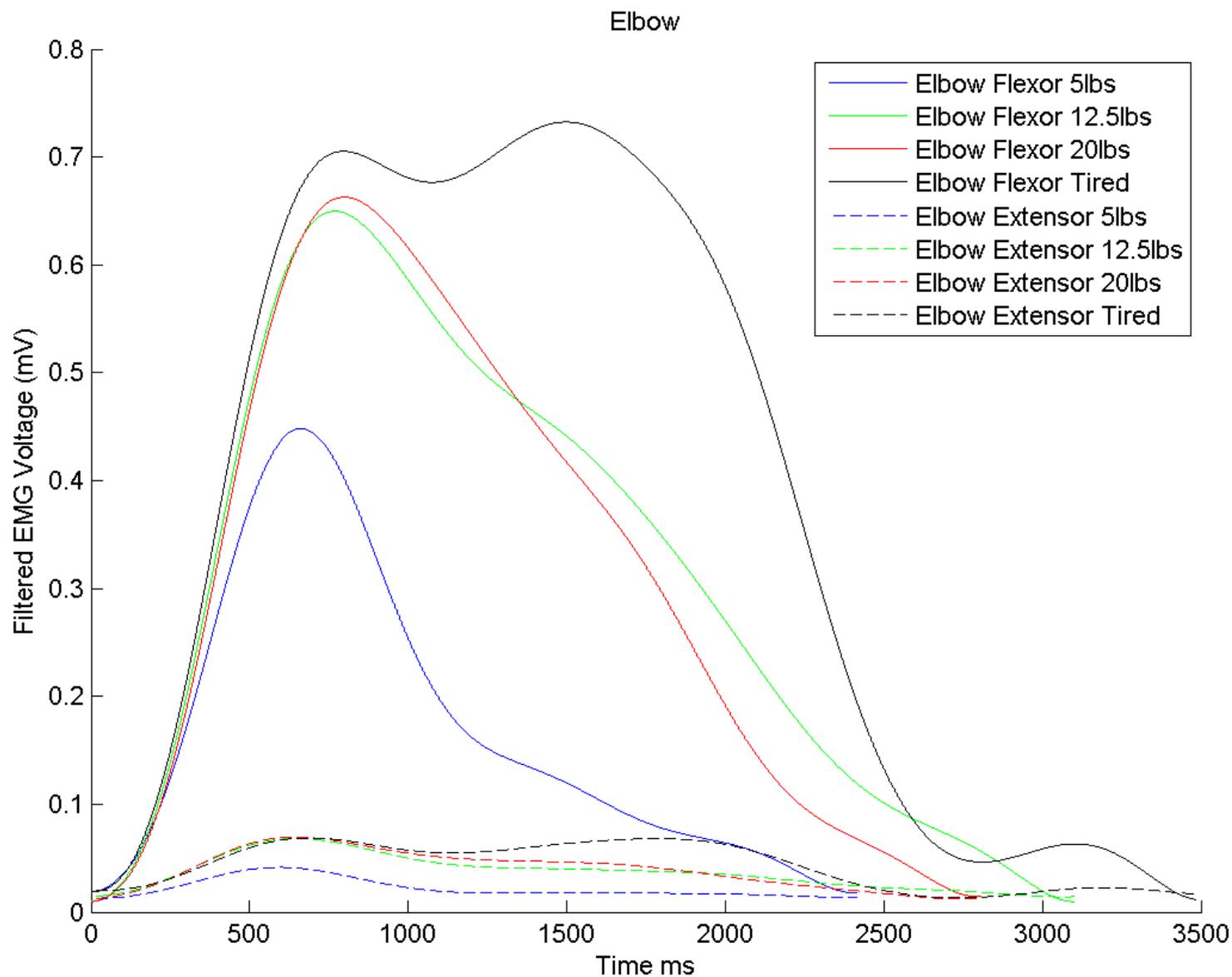
Muscle Modeling

- Compare estimated muscle activations to measured EMG data

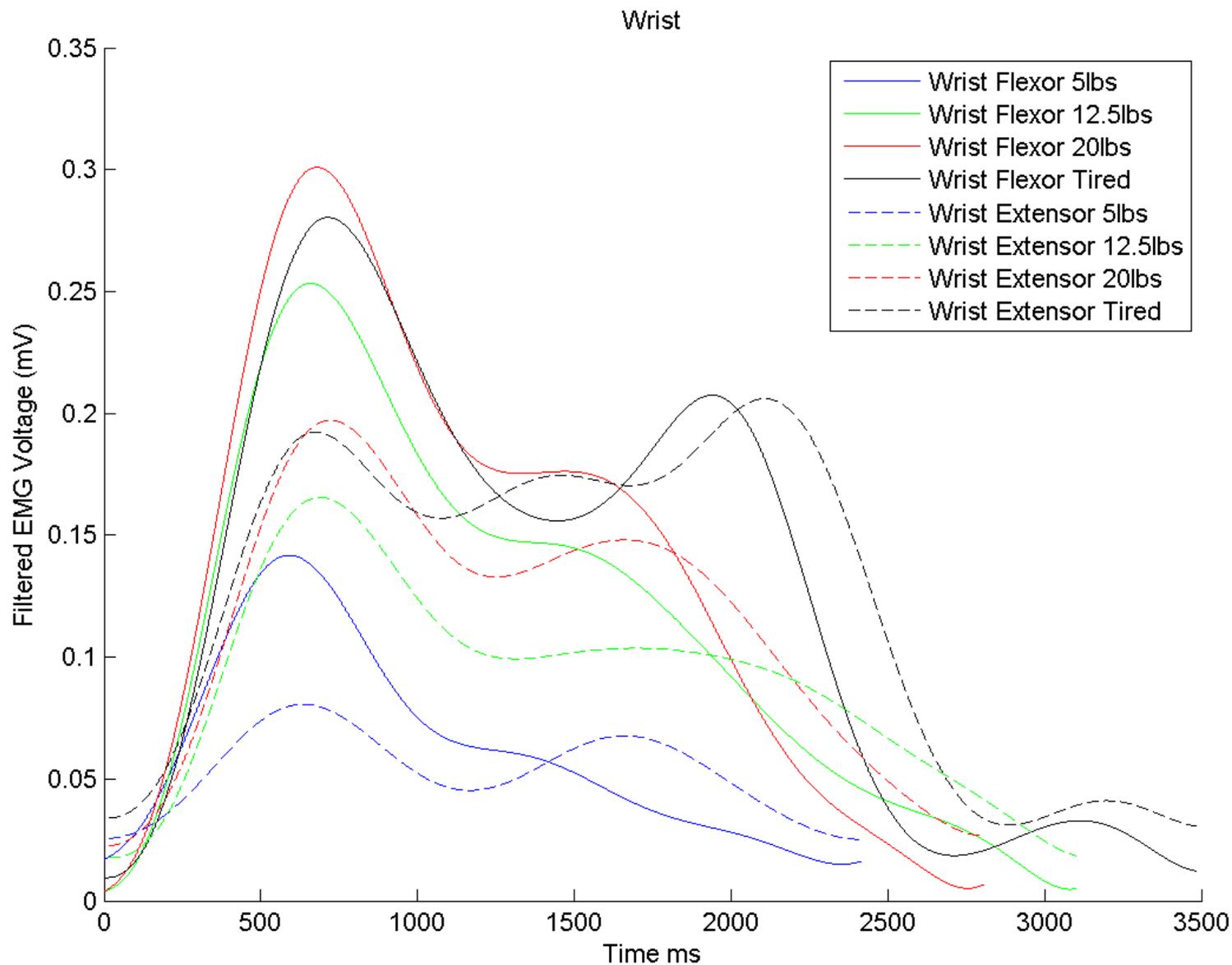
Bibliography

- [1]- NASA. Human Integration handbook. Technical report 2010.
- [2]- Human Engineering Design Data Digest. Department of Defense, Human Factors Engineering. 2000
- [3]- A Model of the Upper Extremity for Simulating Musculoskeletal Surgery and Analyzing Neuromuscular Control, 2005. Katherine R. S. Holzbaur, Wendy M. Murray, Scott L. Delp, Annals of Biomedical Engineering, 33:6 (829-840).
- [4]- Scaling of peak moment arms of elbow muscles with upper extremity bone dimensions. Wendy M Murray, Thomas S. Buchanan, Scott L. Delp. Journal of Biomechanics 35 (2002) 19-26
- [5]- The head of shortening and the dynamic constants of muscle, A Hill, 1938, Royal Society of London. Proceedings Series B 126(843) 136-195.
- [6]-Muscle and Tendon: properties, models, scaling, and application to biomechanics and motor control. F. Zajac, 1989. Critical Reviews in Biomedical Engineering, 17(4) 359-411.
- [7]- Musculoskeletal parameters of muscles crossing the shoulder and elbow and the effect of sarcomere length sample size on estimation of optimal muscle length. Joseph Langenderfer, Seth A. Jerabek, Vijay B. Thangamani, John E. Kuhn, Richard E. Hughes. 2004, Clinical Biomechanics 19 664-670.
- [8]- Biodigital Human. Biodigital Systems 2013. Online: <https://www.biodigitalhuman.com/> Retrieved 2013-04-20.
- [9]- Gray's Anatomy (Anatomy: Descriptive and Surgical), Henry Gray, 1858, Public works.
- [10]- Regularity Aspects in Inverse Musculoskeletal Biomechanics, Marie Lund, Fredrik Stahl, Marten Gulliksson, 2008, Numerical Analysis and Applied Mathematics, International Conference.
- [11]- Dynamics Computation of Musculo-Skeletal Human Model Based on Efficient Algorithm for Closed Kinematic Chains. Yoshihiko Nakamura, Katsu Yamane, Ichiro Suzuki and Yusuke Fujita, 2003, Proceedings of the 2nd International Symposium on Adaptive Motion of Animals and Machines, March 4-8 2003.
- [12]- Dynamic simulation of human motion: numerically efficient inclusion of muscle physiology by convex optimization, Goele Pipeleers, Bram Demeulenaere, Ilse Jonkers, Pieter Spaepen, Georges Van der Perre, Arthur Spaepen, Jan Sweversm Joris De Schutter, 2008, Optimal Engineering, 9: 213-238.

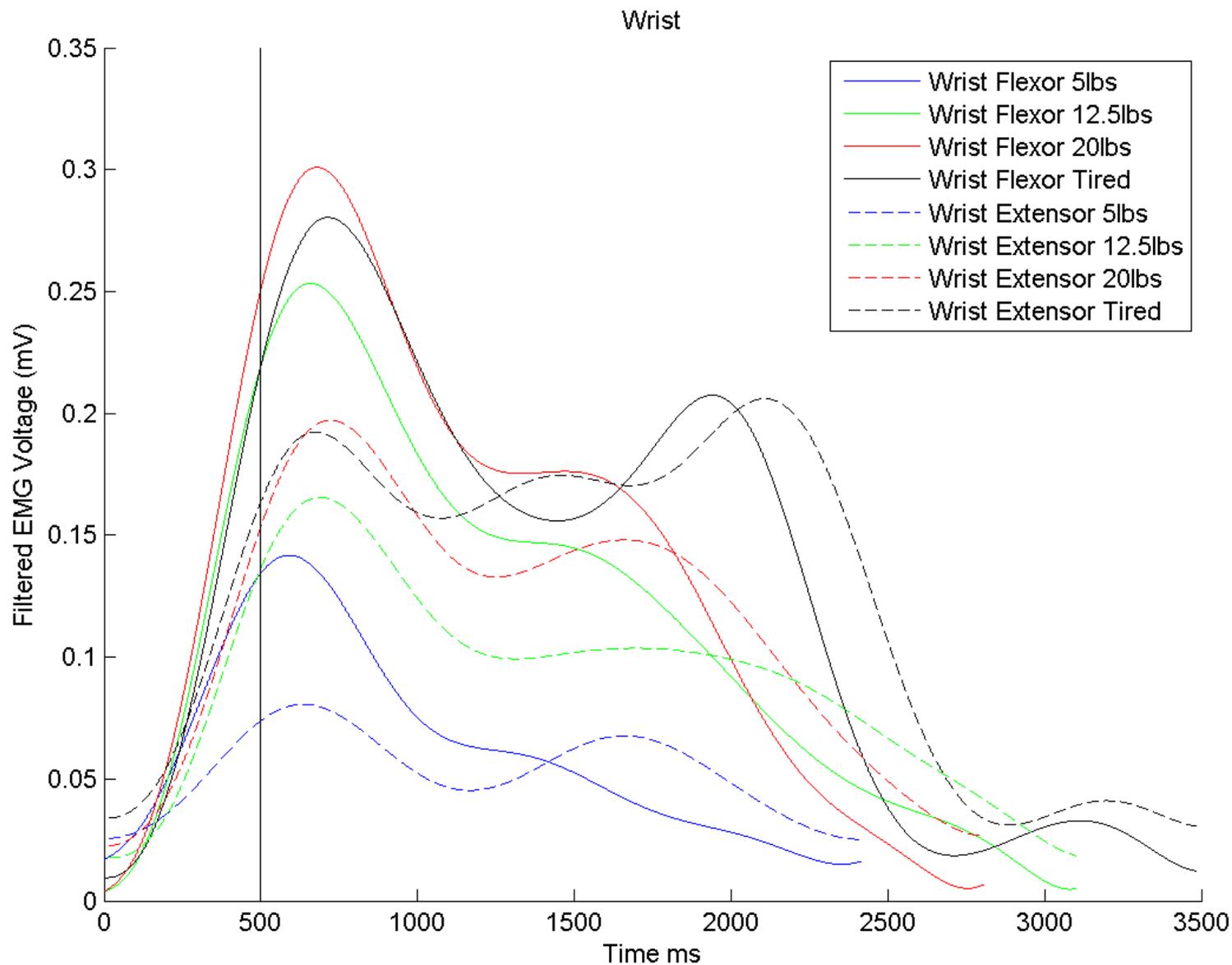
Experimental Results- Elbow- Single Muscle Action



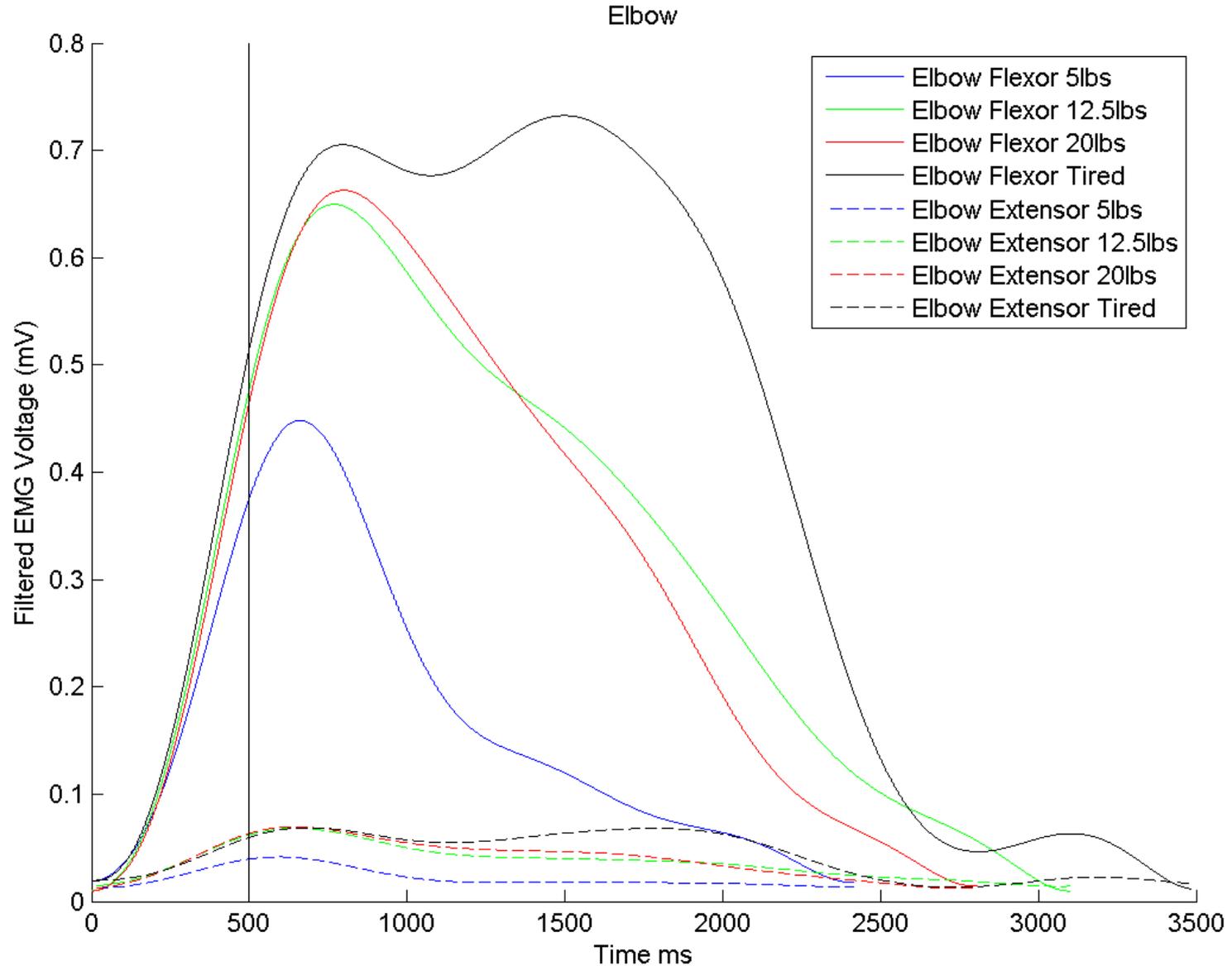
Experimental Results- Wrist- Co-contraction



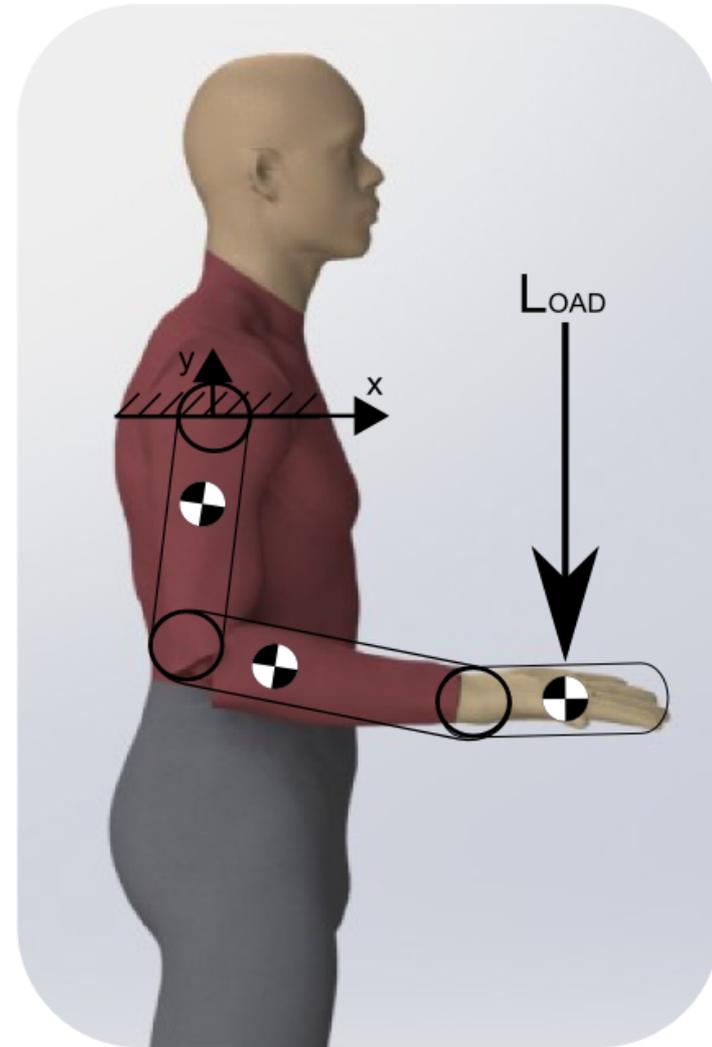
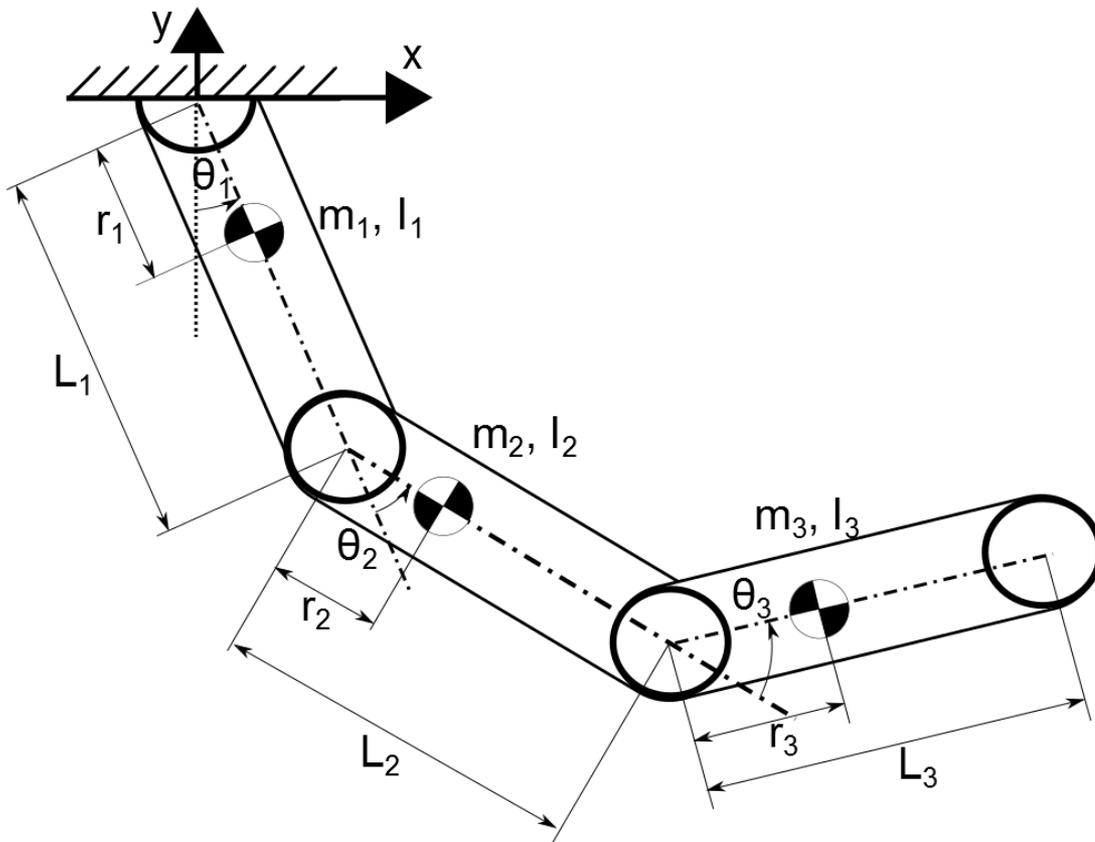
Experimental Results- Wrist- Prediction



Experimental Results: Elbow



Model: Triple Planar Pendulum



NASA. Human Integration handbook. Technical Report 2010.

Human Engineering Design Data Digest. Department of Defense, Human Factors Engineering. 2000

Dynamical Model

- Dynamical Model

$$\begin{aligned}
 & \begin{bmatrix} \alpha + \beta + \gamma + \delta c_3 + \epsilon c_{23} + \zeta L_1 c_2 & \alpha + \beta + \delta c_3 + \epsilon c_{23} + \zeta L_1 c_2 & \alpha + \delta c_3 + \epsilon c_{23} \\ \alpha + \beta + \delta c_3 + \epsilon c_{23} + \zeta L_1 c_2 & \alpha + \beta + \eta c_3 & \alpha + \eta c_3 \\ \alpha + \delta c_3 + \epsilon c_{23} & \alpha + \eta c_3 & \alpha \end{bmatrix} \begin{bmatrix} \ddot{\theta}_1 \\ \ddot{\theta}_2 \\ \ddot{\theta}_3 \end{bmatrix} \\
 + & \begin{bmatrix} -2 \left((\zeta L_1 s_2 + \epsilon s_{23}) \dot{\theta}_2 + \kappa \dot{\theta}_3 \right) & - \left(\zeta L_1 s_2 \dot{\theta}_2 + 2\eta s_3 \dot{\theta}_3 + \epsilon s_{23} (\dot{\theta}_2 + \dot{\theta}_3) \right) & - \left(\kappa \dot{\theta}_3 + \epsilon s_{23} \dot{\theta}_2 \right) \\ (\zeta L_1 s_2 + \epsilon s_{23}) \dot{\theta}_1 - 2\delta s_3 \dot{\theta}_3 & -2\delta s_3 \dot{\theta}_3 & -\delta s_3 \\ \kappa \dot{\theta}_1 + 2\delta s_3 \dot{\theta}_2 & \delta s_3 \dot{\theta}_2 & 0 \end{bmatrix} \begin{bmatrix} \dot{\theta}_1 \\ \dot{\theta}_2 \\ \dot{\theta}_3 \end{bmatrix} \\
 & -g \begin{bmatrix} (L_1 (m_2 + m_3) + m_1 r_1) + \zeta c_{12} + m_3 r_3 c_{123} \\ \zeta c_{12} + m_3 r_3 c_{123} \\ m_3 r_3 c_{123} \end{bmatrix} = \begin{bmatrix} \tau_1 \\ \tau_2 \\ \tau_3 \end{bmatrix}
 \end{aligned}$$

- Where:

$$\begin{aligned}
 \alpha &= I_{3Z} + m_3 r_3^2 & \epsilon &= L_1 m_3 r_3 \\
 \beta &= I_{2Z} + L_2^2 m_3 + m_2 r_2^2 + L_2 m_3 r_3 c_3 & \zeta &= L_2 m_3 + m_2 r_2 \\
 \gamma &= I_{1Z} + L_1^2 m_2 + L_1^2 m_3 + m_1 r_1^2 + L_1 (L_2 m_3 + m_2 r_2) c_2 + L_1 m_3 r_3 c_{23} & \eta &= L_2 m_3 r_3 \\
 \delta &= L_2 m_3 r_3 & \kappa &= \delta s_3 + \epsilon s_{23}
 \end{aligned}$$

Muscle Model

Tendon model:

$$f_t(l_t) = K_t \left[\frac{l_t - l_s}{l_s} \right] f_o$$

Muscle Passive force:

$$f_p(\bar{l}_m) = \frac{2.5}{1 + e^{-12(\bar{l}_m - 1.425)}} f_o$$

Muscular Active force:

$$f_a(a, \bar{l}_m, \dot{\bar{l}}_m) = a f_l(\bar{l}_m) f_v(\dot{\bar{l}}_m) f_o$$

Length-Force relation:

$$f_l(\bar{l}_m) = \left[\frac{1}{1 + e^{-12(\bar{l}_m - 0.6)}} + \frac{1}{1 + e^{12(\bar{l}_m - 1.4)}} - 1 \right]$$

Velocity-Force relation:

$$f_v(\dot{\bar{l}}_m) = \begin{cases} f_{v_{min}} & \dot{\bar{l}}_m < \dot{\bar{l}}_{min} \\ \frac{2}{1 + e^{-6\dot{\bar{l}}_m}} & \dot{\bar{l}}_{min} \leq \dot{\bar{l}}_m \leq \dot{\bar{l}}_{max} \\ f_{v_{max}} & \dot{\bar{l}}_m > \dot{\bar{l}}_{max} \end{cases}$$

where:

$$\begin{aligned} \dot{\bar{l}}_{min} &= -1 & f_{v_{min}} &= \frac{2}{1 + e^6} \\ \dot{\bar{l}}_{max} &= -\frac{1}{6} \ln \left(\frac{2}{1.8} - 1 \right) & f_{v_{max}} &= 1.8 \end{aligned}$$

